

3d electron microscopy in injured rat brain validates white matter microstructure metrics from diffusion MRI

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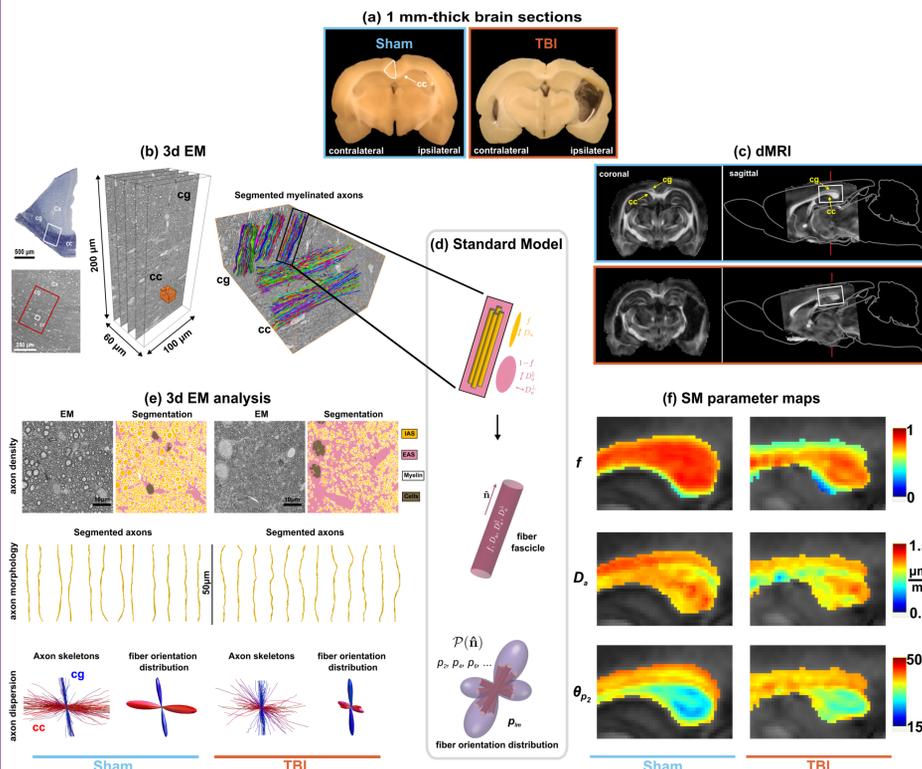


Fig. 1. SM parameter maps reveal specific microstructure properties that correspond to 3d EM.

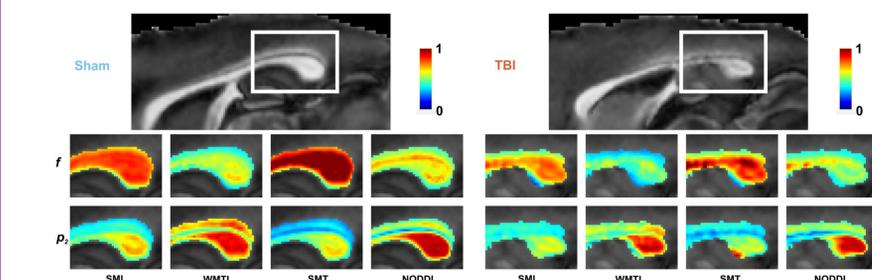


Fig. 2. SM parameter maps obtained using different estimators: WMTI, NODDI, SMT & SMI

Results

- Fig. 1e** shows reduction of axonal density, changes in axon morphology (diameter reduction, increased beading & undulation), and increase in dispersion for the TBI sample. Remarkably, these microstructural changes are also detected non-invasively by ex vivo MRI, as shown on the SM maps in **Fig. 1f** for f , D_a , and θ_{p_2} , and **Fig. 2**.
- Correspondence between 3d EM and dMRI metrics are observed in **Fig. 3** and **Fig. 4**:
 - Intra-axonal water fraction f** ^{21,22}: SMI, WMTI and SMT show significant correlations with 3d EM f and don't correlated with \bar{D}_a , and θ metrics, showing specificity.
 - Dispersion angle θ_{p_2}** ^{5,25}: All methods show significant correlations 3d EM θ , but only SMI, SMT and NODDI show specificity, as WMTI θ_{p_2} also correlates with histological f .
 - Intra-axonal diffusivity D_a** : SMI, WMTI and SMT show correlations with predicted \bar{D}_a from the axial tortuosity and undulation of the axons, assuming free diffusivity for perfect cylinders, in agreement with MC studies^{20,23,24}. Only SMI D_a shows specificity.
 - Radial extra-axonal diffusivity D_e^\perp** : the positive correlation between 3d EM f with SMI D_e^\perp contradicts the tortuosity relation^{26,27} used by NODDI and SMT. Using functional relations between D_e^\perp and f is unjustified, and they rather should be estimated independently, particularly in pathological conditions.

dMRI	SMI					WMTI					SMT					NODDI						
	f	θ_{p_2}	D_a	D_e^\parallel	D_e^\perp	f	θ_{p_2}	D_a	D_e^\parallel	D_e^\perp	f	θ_{p_2}	D_a	D_e^\parallel	D_e^\perp	f	θ_{p_2}	D_a	D_e^\parallel	D_e^\perp	f_w	
f	0.60*	-0.18	0.29	0.37	0.51*	0.43	-0.41	0.40	0.48*	0.36	0.61*	0.20	0.60*	-0.56*	0.24	-0.22	-0.42	0.54*	0.24	-0.22	-0.42	0.54*
θ	0.04	0.86*	-0.35	-0.26	0.11	-0.06	0.52*	-0.42	-0.55*	0.31	0.05	0.48*	-0.08	-0.08	0.40	0.69*	-0.29	0.02	0.40	0.69*	-0.29	0.02
\bar{D}_a	0.35	-0.19	0.55*	0.34	0.35	0.24	-0.30	0.43	0.36	0.39	0.25	0.04	0.45	-0.12	-0.25	-0.30	-0.01	0.41	-0.25	-0.30	-0.01	0.41
$2r$	0.08	-0.28	0.49*	0.02	0.10	0.14	-0.07	0.35	0.17	0.17	-0.02	-0.17	0.09	0.01	-0.22	-0.25	0.08	0.12	-0.22	-0.25	0.08	0.12

Fig. 3. Pearson correlations between 3d EM histology derived metrics (rows) and dMRI estimated SM parameters (columns) for the different estimators. Significant correlation ($p < 0.05$) are highlighted in **bold**, while * indicates that significance remains after adjusting for multiple comparisons using the false discovery rate.

Conclusions

- We used 3d EM derived metrics on sham and injured rat brains to validate SM parameters from four publicly available estimators: WMTI, NODDI, SMT and SMI.
- All SM estimators provide SM parameters that correlate significantly ($p < 0.05$) with their histological counterparts (except for NODDI's f), indicating sensitivity.
- SMI shows the highest specificity by presenting smallest cross-correlations with other, non-corresponding histological features.

References

1 Novikov DS et al. NMR Biomed. 32 4 (2019); 2 Alexander DC et al. NMR Biomed. 32 4 (2019); 3 Jelescu IO and Budde MD. Front. Physics 5 (2017); 4 Salo RA et al. Neuroimage 172 (2018); 5 Salo RA et al. Neuroimage 225 (2021); 6 Veraart J et al. Neuroimage 142 (2016); 7 Kellner E et al. Magn. Reson. Med. 76 5 (2016); 8 Tustison NJ et al. IEEE Trans. Med. Imaging 29 6 (2010); 9 Avants BB et al. Med. Image Anal. 12 1 (2008); 10 Jelescu IO et al. Neuroimage 132 (2016); 11 Fieremans E et al. Neuroimage 58 1 (2011); 12 Zhang H et al. Neuroimage 61 4 (2012); 13 Kaden et al. Neuroimage 139 (2016); 14 Reisert M et al. Neuroimage 147 (2017); 15 Novikov DS Neuroimage 174 (2018); 16 Coelho et al. Neuroimage 257 (2022); 17 Abdollahzadeh A et al. Sci Rep 9 1 (2019); 18 Abdollahzadeh A et al. Commun Biol. 4 1 (2021); 19 Lee HH et al. Brain Struct Funct 224 4 (2019); 20 Abdollahzadeh A et al. ISMRM (2023); 21 Jelescu IO et al. Neuroimage 132 (2016); 22 Coronado-Leija R et al. ISMRM (2021); 23 Budde MD et al. Proc Natl Acad Sci. 107 32 (2010); 24 Lee HH. Commun Biol. 3 1 (2020); 25 Schilling KG et al. Neuroimage 165 (2018); 26 Sen et al. Geophysics 46 5 (1981); 27 Zafer A et al. Magn. Reson. Med. 33 5 (1995);

Introduction

- Biophysical modeling of diffusion MRI¹⁻³ (dMRI) offers the exciting potential of bridging the gap between the macroscopic MRI resolution and microscopic cellular features, effectively turning the MRI scanner into a noninvasive *in vivo* microscope.
- In brain white matter (WM), the Standard Model (SM) interprets the dMRI signal in terms of axon dispersion, intra- and extra-axonal water fractions and diffusivities, see **Fig. 1d**. SM is described by parameters f , D_a , D_e^\parallel , D_e^\perp , and the FOD $\mathcal{P}(\hat{n})$.
- In this work, we perform a comprehensive histological validation of the sensitivity and specificity of the SM parameters, by characterizing WM microstructure in sham and injured rat brains using *ex vivo* dMRI and 3d electron microscopy (EM).

Methods

- Animal preparation**^{4,5}. Traumatic Brain Injury (TBI) was induced by a lateral fluid-percussion injury in three adult rats, while two rats went through a sham-operation that included all surgical procedures except the impact, **Fig. 1a**.
- dMRI imaging**: *Ex vivo* dMRI data ($150 \times 150 \times 150 \mu\text{m}^3$) was acquired on a 9.4T magnet at room temperature, 21°C, using 42 diffusion gradient directions for $b = 2, 3$, and 4 $\text{ms}/\mu\text{m}^2$; with 3 non-diffusion weighted images. $\delta/\Delta = 6/11.5$ ms, $\text{TR}/\text{TE} = 1000/35$ ms. FA maps for sham and TBI rats are shown in **Fig. 1c**.
- dMRI processing**: Images were denoised⁶, corrected for Gibbs-ringing⁷, B1 inhomogeneities⁸ and motion distortions⁹. SM parameters were obtained using four different estimators that handle the known degeneracies of the problem¹⁰: WMTI¹¹, NODDI¹², SMT¹³ and SMI¹⁴⁻¹⁶. SM maps differences are shown in **Fig. 2**.
- 3d EM imaging and segmentation**: Ten WM samples, two from each rat, were prepared for serial block-face-scanning electron microscopy imaging^{4,5}, as shown in **Fig. 1b**. Large tissue volumes of $200 \times 100 \times 65 \mu\text{m}^3$ were imaged with resolution of $50 \times 50 \times 50 \text{ nm}^3$. Myelin and myelinated axons were automatically segmented using the deep-learning pipeline DeepACSON^{17,18}.
- Microstructural metrics derived from 3d EM**: From 3d EM segmentations, the intra-axon volume fraction f was computed. From the segmented 3d axons¹⁹, the diameter, the axial tortuosity Λ_\parallel from the cross-sectional area variations derived in ref²⁰, dispersion angle θ , and fiber orientation distribution with their rotational invariants p_i were computed. Undulation based dispersion angle θ_u was computed by first aligning all axons to the z-axis. p_2 is approximately related to the dispersion angle^{15,19} by $\cos^2 \theta \approx \cos^2 \theta_{p_2} = \frac{2p_2 + 1}{3}$.

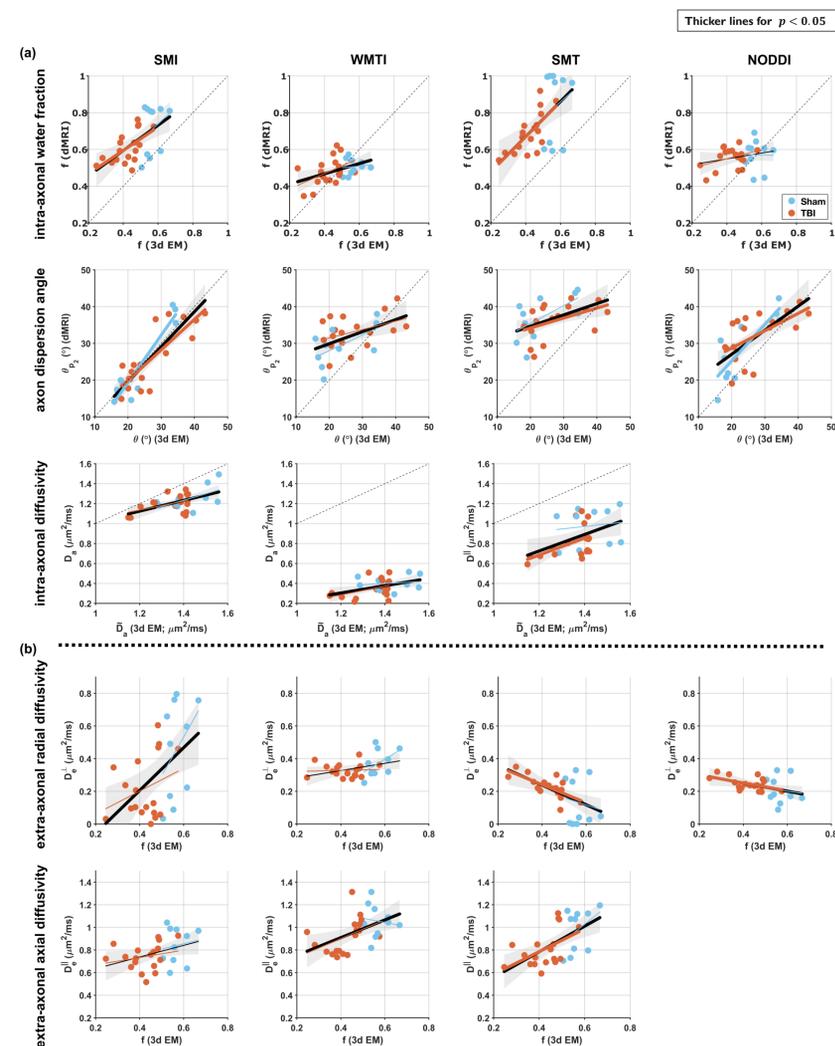


Fig. 4. Scatter plots for dMRI derived parameters against histology metrics. (a) SM parameters f , D_a , and θ_{p_2} from SMI, WMTI, SMT, and NODDI compared against their corresponding 3d EM metrics. (b) SM extra-axonal diffusivities D_e^\parallel , D_e^\perp compared against histological f .

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