

Problem and Motivations

- Fast data acquisition in Magnetic Resonance Imaging (MRI) is vastly in demand and scan time directly depends on the number of acquired k-space samples.

Current Issues:

- The clinical gold standard GRAPPA method [1] generates noisy reconstruction in highly accelerated data acquisition.
- Deep learning-based MRI reconstruction approaches [2,3,4,5] need to learn from massive datasets through the training processes and can't handle k-space data with different undersampling patterns, and different number of coils. Their networks must be trained from scratch every time with new training datasets, acquired under new configurations.

Proposed Solution:

- In this work, we developed the generalized deep neural network-based method without any training data involved using convolutional neural network for parallel MRI reconstruction. Our method can be categorized among the unsupervised energy-based methods [6,7].
- Our method only needs the single undersampled multi-coil k-space data for reconstruction.
- Two deep loss functions including non-regularized and regularized are proposed for parallel MRI reconstruction.

NLDpMRI: Main Idea

Our proposed method (NLDpMRI) includes U-net [8] convolutional network with deep loss function. In our reconstruction process, we optimize the loss function over the network parameters.

The following equations are the proposed non-regularized and regularized deep loss functions:

$$\hat{\theta} = \operatorname{argmin}_{\theta} \|PFS_l x_{\theta} - d_u\|_2^2$$

$$\hat{\theta} = \operatorname{argmin}_{\theta} \|PFS_l x_{\theta} - d_u\|_2^2 + \lambda \|\theta\|_2$$

θ represents the network parameters
 x_{θ} is the network output with parameters θ
 $x_{\hat{\theta}}$ is the MR image to be reconstructed
 d_u is the undersampled k-space data
 P is a k-space undersampling pattern mask
 F is the Fourier transform operator
 S_l represents coil sensitivity maps
 l is the total number of coils

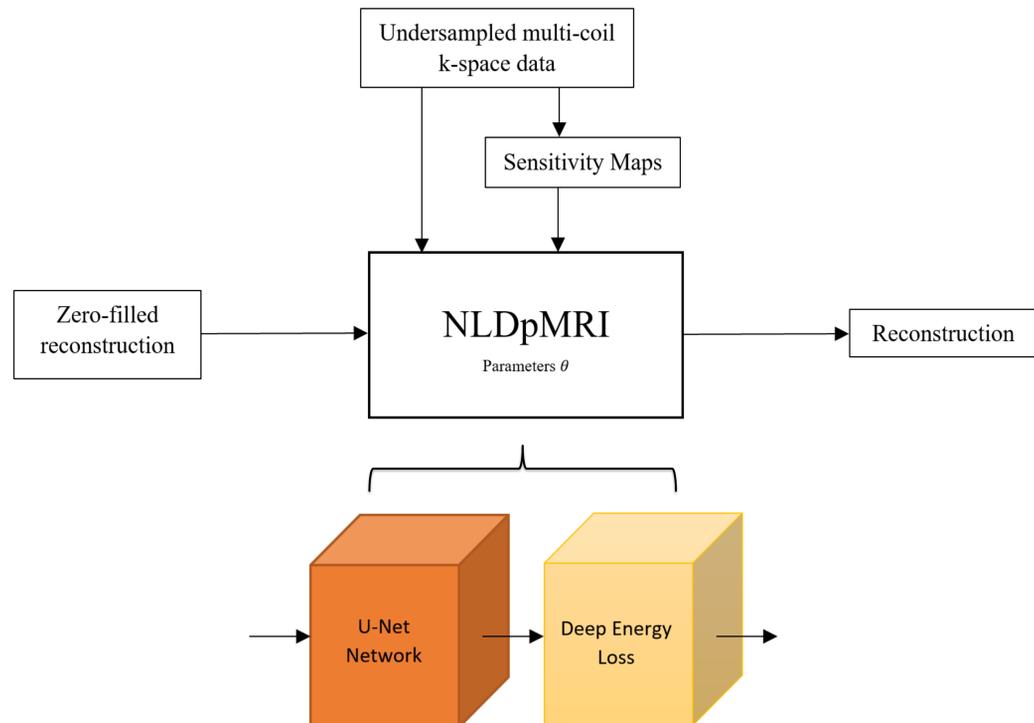


FIG 1. NLDpMRI Framework

NLDpMRI Reconstruction

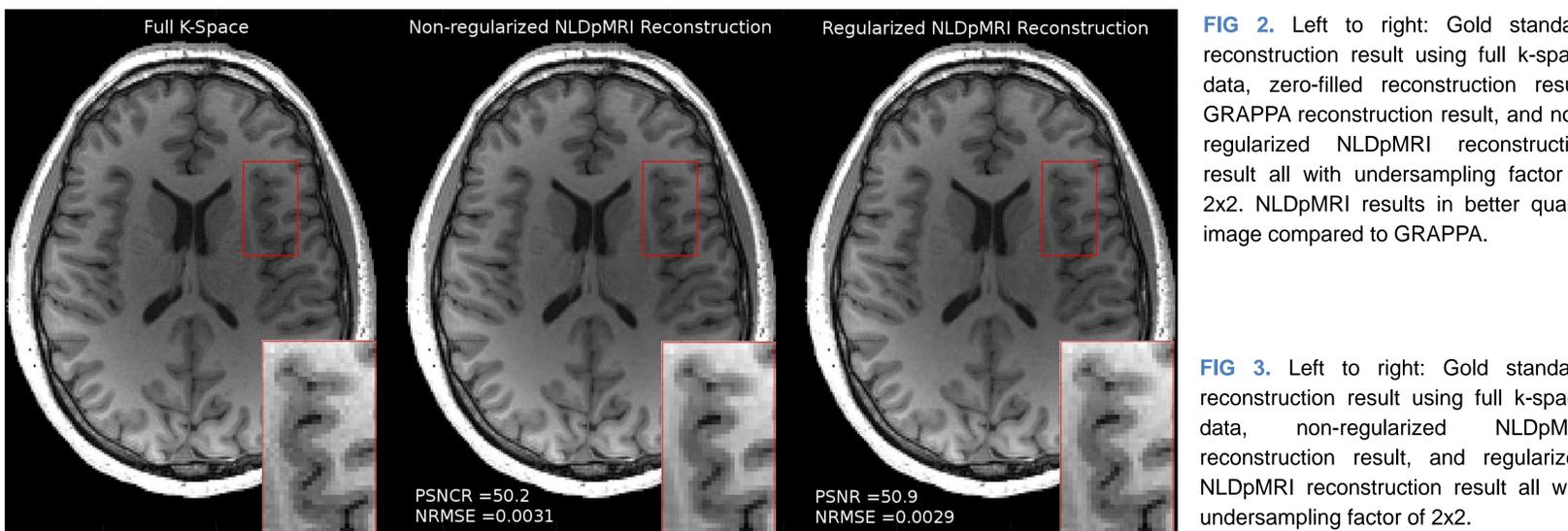
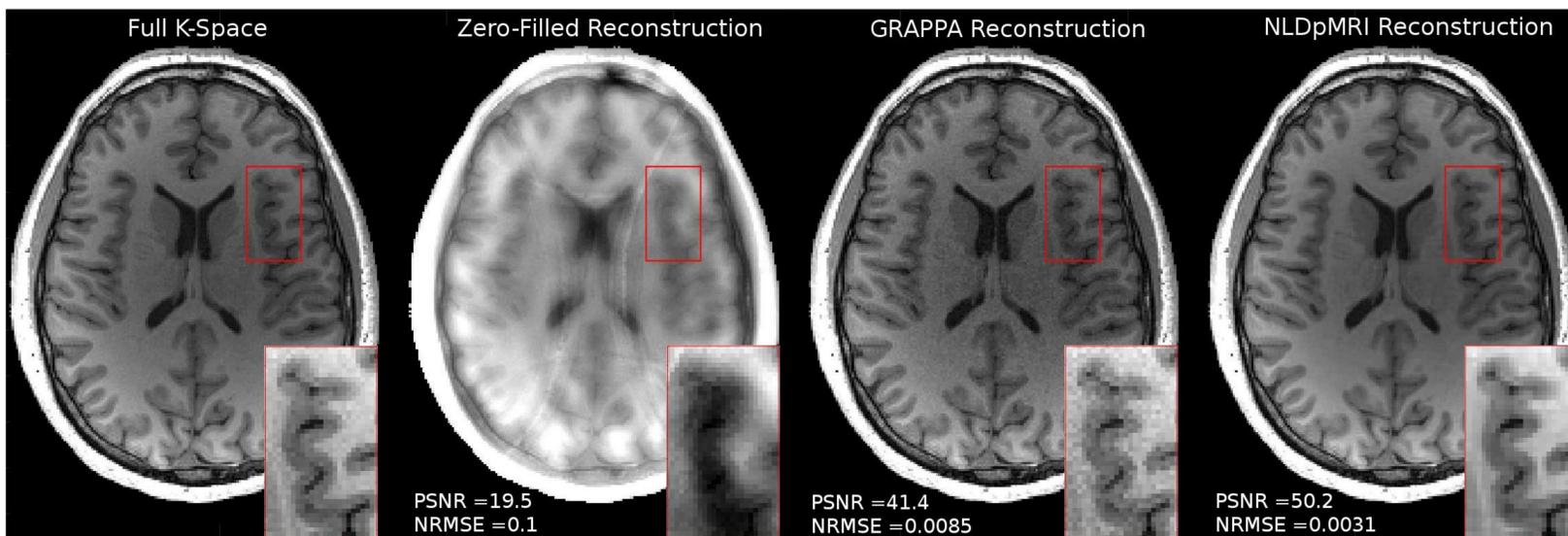


FIG 2. Left to right: Gold standard reconstruction result using full k-space data, zero-filled reconstruction result, GRAPPA reconstruction result, and non-regularized NLDpMRI reconstruction result all with undersampling factor of 2x2. NLDpMRI results in better quality image compared to GRAPPA.

FIG 3. Left to right: Gold standard reconstruction result using full k-space data, non-regularized NLDpMRI reconstruction result, and regularized NLDpMRI reconstruction result all with undersampling factor of 2x2.

Conclusion

- We propose a generalized method to solve MRI parallel image reconstruction problem using deep neural networks without any training data involved.
- The proposed approach eliminates the need to collect massive datasets for training purposes, any form of normalization, and transfer learning techniques.
- Experimental results on real MRI acquisitions show that our proposed method outperforms the clinical gold standard GRAPPA method [1].

References

- Griswold *et al.* 2002. *Magn Reson Med*, **47**(6); 1202-1210.
- Wang *et al.* 2016. *IEEE 13th ISBI*, 514-17.
- Schlemper *et al.* 2018. *IEEE Trans Med Imaging*, **37**(2);491-503.
- Hammernik *et al.* 2018. *Magn Reson Med*, **79**(6); 3055-3071.
- Zhu *et al.* 2018. *Nature*, 555(7697):487.
- Golts *et al.* 2018. arXiv preprint arXiv:1805.12355.
- Ulyanov *et al.* 2018. *Proc of the IEEE Conf CVPR*, 18.
- Ronneberger *et al.* 2015. *MICCAI*, 234-241.

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