



Development of new concept antenna (Mono-Dipole) array for human head imaging at 10.5T

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Motivation and Objective: As a transmitter, a 16 channel (CH) dipole head array is desirable above 7T, however, it is difficult to achieve this high channel count due to coupling [1-3]. Shortening the length of the dipole is also required for human head applications [4, 5]. We explore the potential of a novel 16 CH Mono-Dipole head array to achieve improved B_1^+ field uniformity and intra-element decoupling. To investigate this, we first compared an 8 CH end-loaded dipole array and a Mono-Dipole array in simulation and verified B_1^+ experimentally [6]. We then compared arrays of 16 CH Mono-Dipole and closer fitting Stripline arrays for achievable B_1^+ field efficiency at 10.5T.

Methods: The 16 CH transceiver Mono-Dipole head array is shown in Fig. 1. The coil was effectively shortened to a common RF ground using 680 pF capacitors in Fig. 2. Floating cable traps were used to suppress the cable sheath currents [7].

Electromagnetic simulations were performed in XFDTD (REMGCOM, State College, PA) to calculate the B_1^+ field (normalized to 1 W). The B_1^+ efficiency was initially compared with 8 CH Dipole array and Mono-Dipole array of the same dimensions (Fig. 3). Transmit B_1^+ profiles obtained using an actual flip angle imaging (AFI) sequence for a cylindrical phantom (17 cm diameter, 30.5 cm height) are also shown in Fig 3. The phantom has uniform electrical properties ($\sigma = 0.6$ S/m, $\epsilon_r = 49$). Fig. 4 shows the experimentally acquired individual transmit fields of the Mono-Dipole array. Fig. 5 shows the experimental results of the comparison between the arrays of 16 CH Stripline (20 × 22 cm²) and Mono-Dipole (24 × 24 cm²). Fig. 6 shows the simulation result of the 16 CH Mono-Dipole array with a human model (Duke).

Results: Excellent agreement between simulations and experiments (within 10%) was achieved for the highest B_1^+ values among the 8 CH end-loaded dipole and the Mono-Dipole arrays in Fig. 2. Individual element performance of the 16 CH Mono-Dipole array is shown in Fig. 3. Coupling of the 16CH Mono-Dipole array is on the order of -9 ~ -11 dB between the next nearest neighbors. From AFI imaging, the transmit efficiency of the Stripline array (0.51 $\mu\text{T}/\sqrt{\text{W}}$) was lower than the Mono-Dipole array (0.59 $\mu\text{T}/\sqrt{\text{W}}$) in Fig. 5. Even though the dimension of Stripline array has a 20% smaller area than the Mono-dipole array, Mono-Dipole array shows higher B_1^+ efficiency compared to the Stripline array.

Conclusion: Improved decoupling between channels is observed in the Mono-Dipole arrays. For the 16 CH Mono-Dipole array, phase shimming between elements is required for optimized results. We observed that 16 CH Mono-Dipole head antenna array has potential advantages for whole head coverage at 10.5T.

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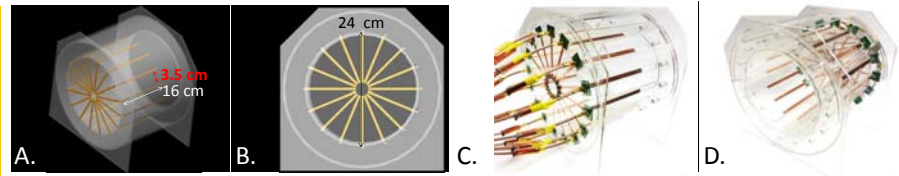


Figure 1. 3D CAD Rendering (A and B) and Photographs (C and D) of the 16 CH Mono-Dipole array

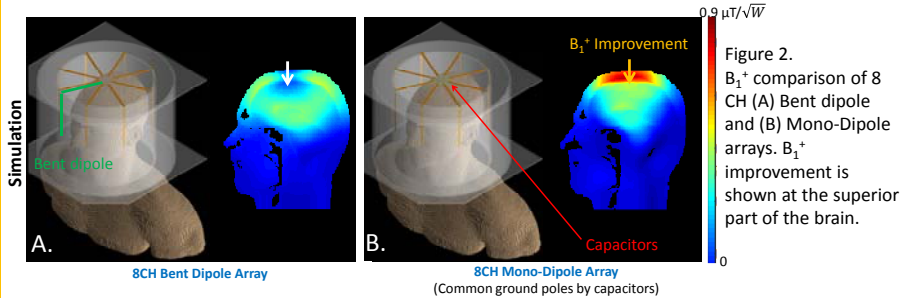


Figure 2. B_1^+ comparison of 8 CH (A) Bent dipole and (B) Mono-Dipole arrays. B_1^+ improvement is shown at the superior part of the brain.

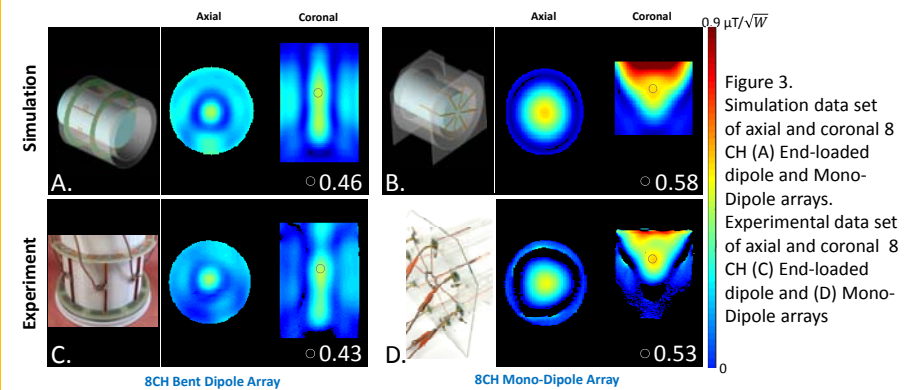


Figure 3. Simulation data set of axial and coronal 8 CH (A) End-loaded dipole and Mono-Dipole arrays. Experimental data set of axial and coronal 8 CH (C) End-loaded dipole and (D) Mono-Dipole arrays

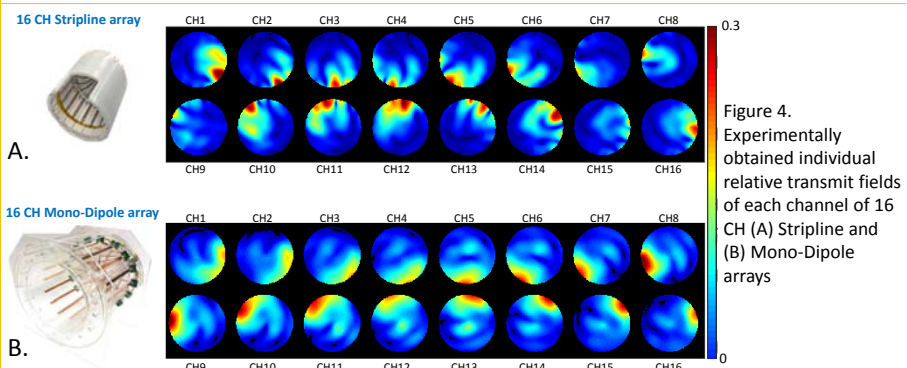


Figure 4. Experimentally obtained individual relative transmit fields of each channel of 16 CH (A) Stripline and (B) Mono-Dipole arrays

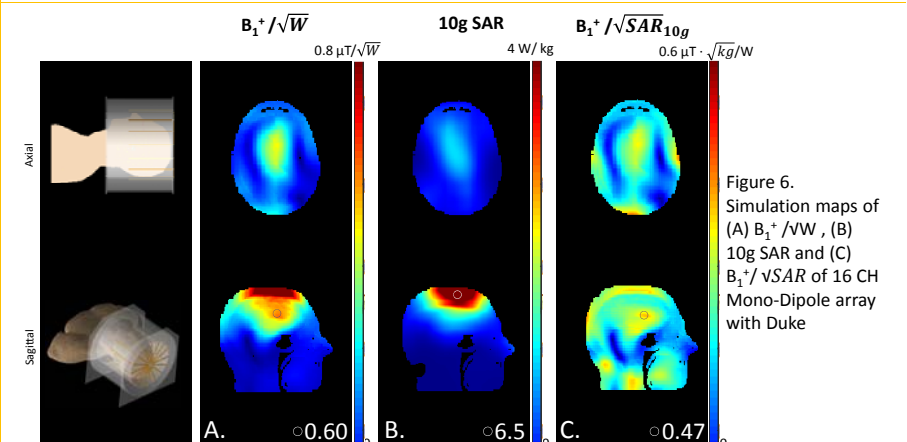


Figure 6. Simulation maps of (A) B_1^+ / \sqrt{W} , (B) 10g SAR and (C) $B_1^+ / \sqrt{SAR_{10g}}$ of 16 CH Mono-Dipole array with Duke

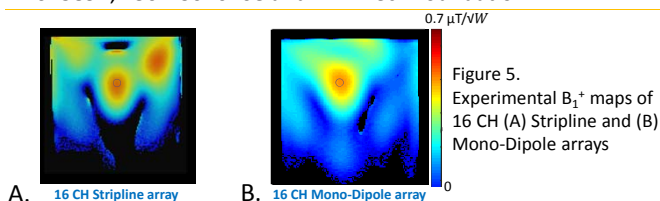


Figure 5. Experimental B_1^+ maps of 16 CH (A) Stripline and (B) Mono-Dipole arrays

A. 16 CH Stripline array B. 16 CH Mono-Dipole array