

Background

- ❑ Motion artifacts are problematic for acquiring diagnostic quality MRI in children and other uncooperative patient groups¹.
- ❑ Large motion also changes the B_0 field distribution, which is a further source of artifacts, especially with longer echo times and high magnetic field strengths².
- ❑ FID navigators (FIDnavs) can rapidly detect head movement³ and have been shown to encode both rigid-body motion⁴ and low-order field information⁵.
- ❑ In this work, we propose an extension to our previously proposed FIDnav framework⁶ to simultaneously estimate head motion and spatiotemporal variations in the B_0 field using simulation of the underlying acquisition physics and a model of the coil sensitivity profiles (CSPs) and first-order field variations.

Theory

- ❑ The FIDnav signal from the j th channel at time τ may be represented as:

$$y_j(\tau) = \int_v s_j(x) \cdot \rho(x; \tau) \cdot \exp(i2\pi\gamma\Delta B_0(x)\tau) dx$$

$s_j(x)$ complex CSP of the j th coil
 $\rho(x; \tau)$ effective spin density of the object
 $\Delta B_0(x)$ field inhomogeneity at position x

- ❑ Spatiotemporal changes in the B_0 field due to the changing magnetic susceptibility distribution can be represented by a series of spherical harmonic basis functions:

$$B_0(x, t) = \beta(x)b(t)$$

- ❑ A forward model of the complex FIDnavs may be constructed using simulated motion and field changes. Given complex FIDnav measurements, the underlying rigid-body motion parameters ($n=6$) and low-order field changes ($n=4$) may be estimated for each TR (Fig. 1).

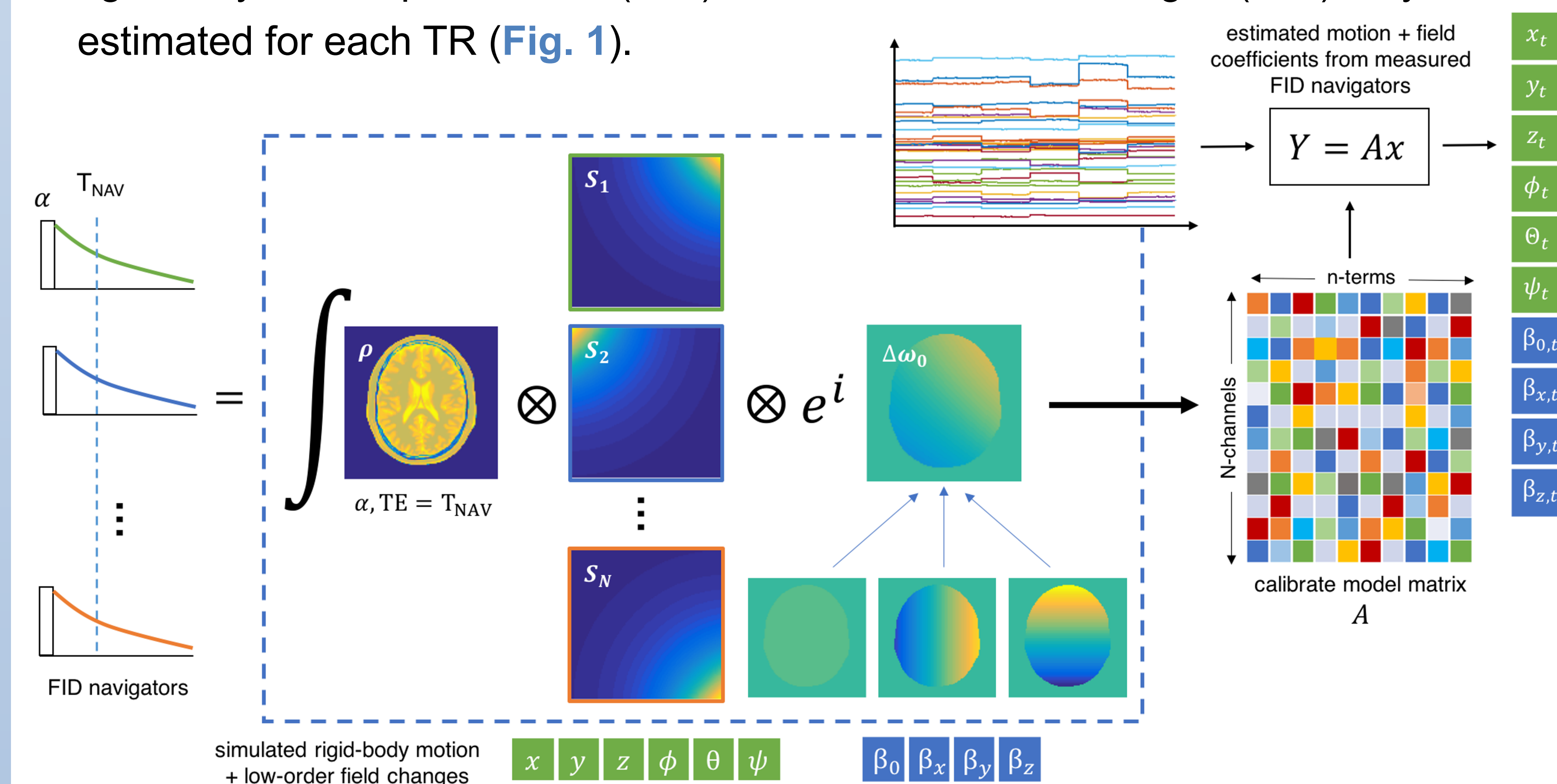


FIG 1. Schematic showing extended FIDnav motion and field measurement framework

Phantom Validation

- ❑ A pineapple was scanned at 3T using a 32-channel head coil. FIDnavs were acquired while first-order shim currents were modified from -4 to $4 \mu\text{Tm}^{-1}$.
- ❑ A reference scan ($\text{TE} = T_{\text{FID}}$) was also acquired on the surface and body coils for estimation of the CSPs and proton distribution. CSPs were extrapolated by fitting a biharmonic smoothing spline to sparse points within the measured data.
- ❑ Complex FIDnavs were generated for step changes of $1 \text{ mm}^\circ/\mu\text{Tm}^{-1}$ by simulating motion of the coils and changes in the field basis functions to compute A .
- ❑ The complex inverse problem was solved via a weighted least-squares fit with a phase constraint⁷ on the real-valued motion and field parameters x .
- ❑ FIDnav field estimates achieved mean absolute errors of $0.07 \pm 0.04 \mu\text{Tm}^{-1}$ with motion estimation errors of $0.06 \pm 0.04 \text{ mm}$ and $0.06 \pm 0.05^\circ$ (Fig. 2).

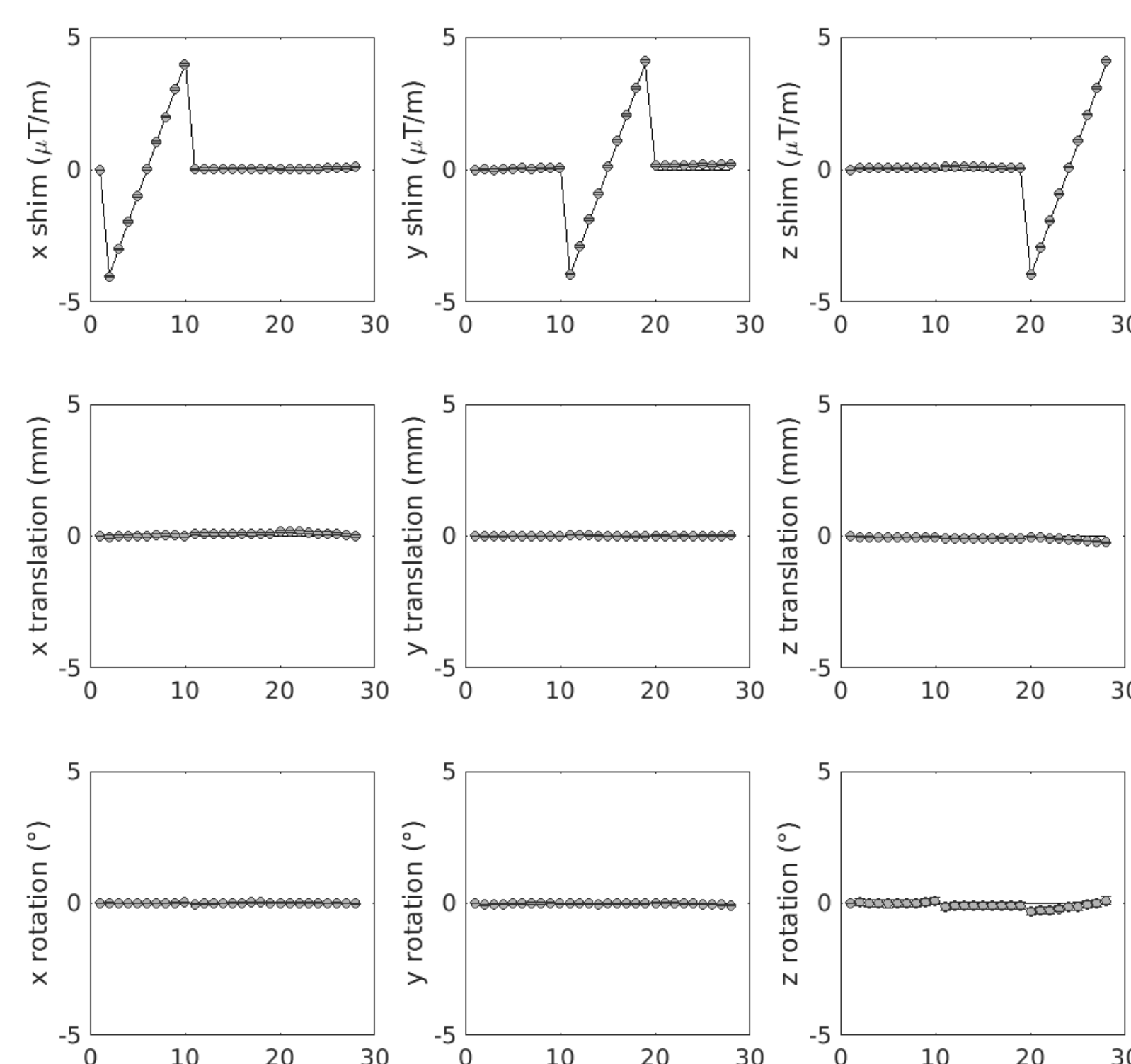


FIG 2. Shim current changes and estimated field and motion parameters from FIDnavs

In Vivo Validation

- ❑ A volunteer was scanned at 3T using a 32-channel head coil. Six sagittal FID-navigated multi-echo 3D FLASH scans were acquired, while the subject moved their head to various poses (up-down-left-right) between each scan.
- ❑ Ground-truth motion parameters were computed via co-registration of the reconstructed images.
- ❑ Ground-truth field maps were calculated in head frame of reference from the phase difference of the registered multi-echo complex data. First-order spherical harmonic functions were fit to the measured ΔB_0 maps within the brain region.

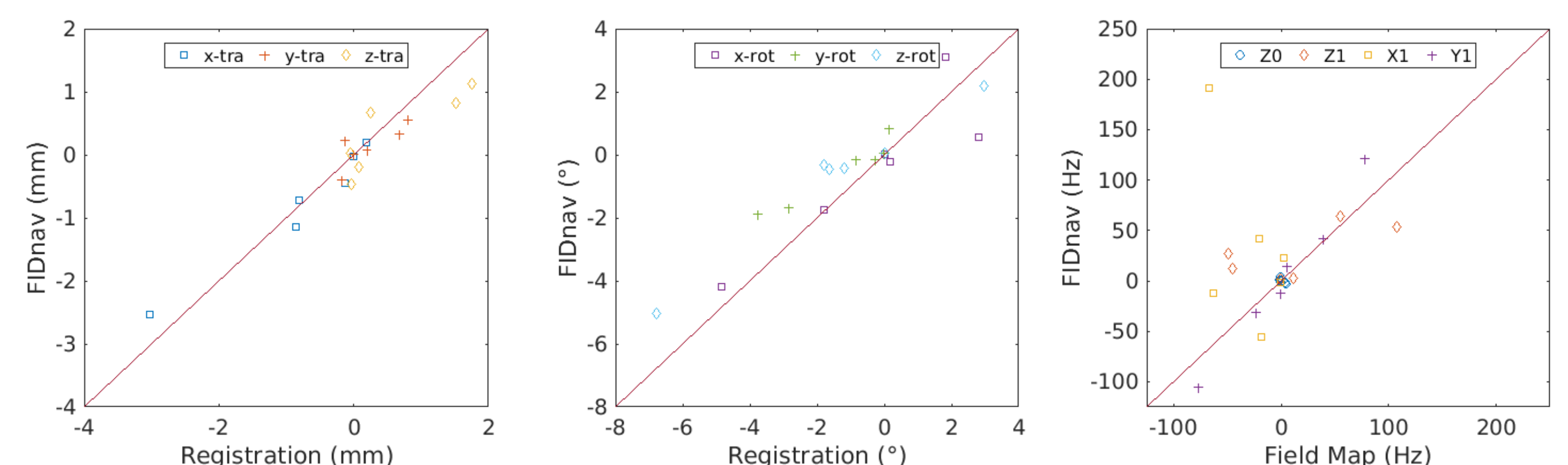


FIG 3. Comparison of FIDnav translational, rotational and field estimates and ground-truth motion and fitted field coefficients at each position

- ❑ FIDnav motion estimates achieved mean absolute errors of $0.29 \pm 0.17 \text{ mm}$ and $0.85 \pm 0.65^\circ$ for maximum changes of 3 mm and 7° (Fig. 3).
- ❑ ΔB_0 maps modelled using the predicted first-order field coefficients from the FIDnavs were in good agreement with the measured field maps (Fig. 4).
- ❑ NRMSE between fitted and measured field maps was 4.0% compared to 4.8% for FIDnav predictions.

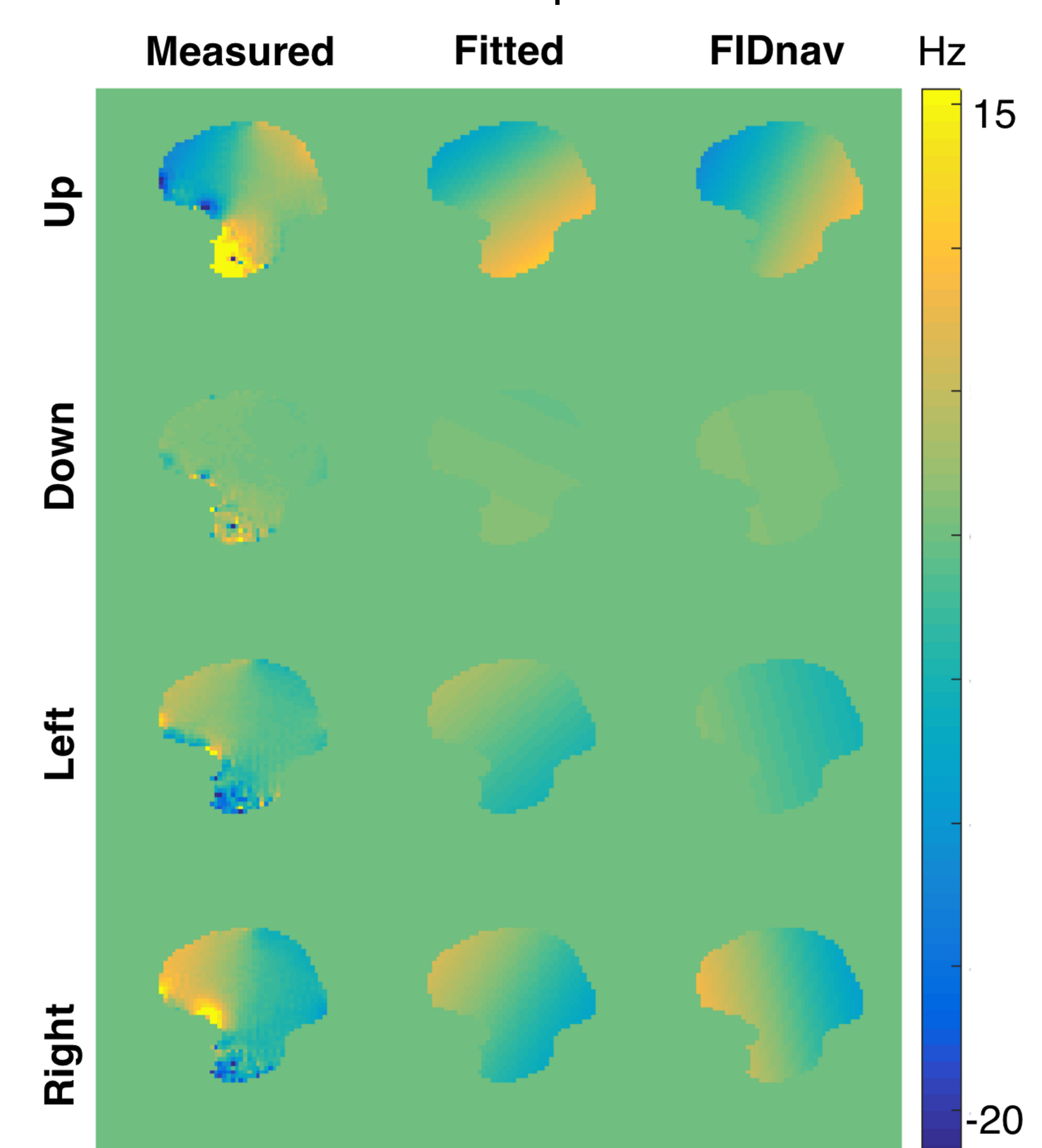


FIG 4. Comparison of measured, fitted and FIDnav-based field maps for each motion

Discussion

- ❑ The proposed approach can simultaneously estimate head pose and related spatiotemporal ΔB_0 field changes from complex FIDnavs with good accuracy.
- ❑ There exists a complex relationship between head pose and B_0 field inhomogeneity distribution². Future iterations could investigate higher-order changes or incorporate explicit modelling of predicted field changes with motion due to the changing orientation of the head relative to the main magnetic field⁸.
- ❑ Higher channel-count coil arrays may facilitate estimation of second-order field changes due to the larger number of unknown parameters.
- ❑ FIDnavs can be inserted into virtually any sequence with minimal time penalty and are a promising method for retrospective correction of motion and ΔB_0 artifacts as well as real-time FOV steering and shimming.

References

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This research was supported in part by the following NIH grant awards:

R01 EB019483, **R01 NS079788** and **R44 MH086984**.